# Plastic compression for generating optimized in vitro skin equivalents

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# Objective

*In vitro* skin equivalents are proven to be useful as both skin grafts and *in vitro* test systems. However, a major drawback during cultivation of the skin equivalents is a contraction up to 70%. In clinical application this results in extensive scarring. Further, the insufficient stability of the test systems limits cultivation to just a few days. Thus, the investigation of many biological processes that occur over a period of weeks is not possible. Hence, we established plastic compression of the dermal equivalents to a defined dimension in order to reduce contraction and set up model systems with a bick or period.

# Materials & Methods

We investigated the mechanical properties of a dermal equivalent after plastic compression with linear motion steering. During this process, collagen hydrogels are compressed to an increasing concentration with a defined force, thereby enhancing both the mechanical stability of the hydrogel and the parallel arrangement of the collagen filaments. We developed a system which allows a defined compression and the mechanical characterization of collagen hydrogels.

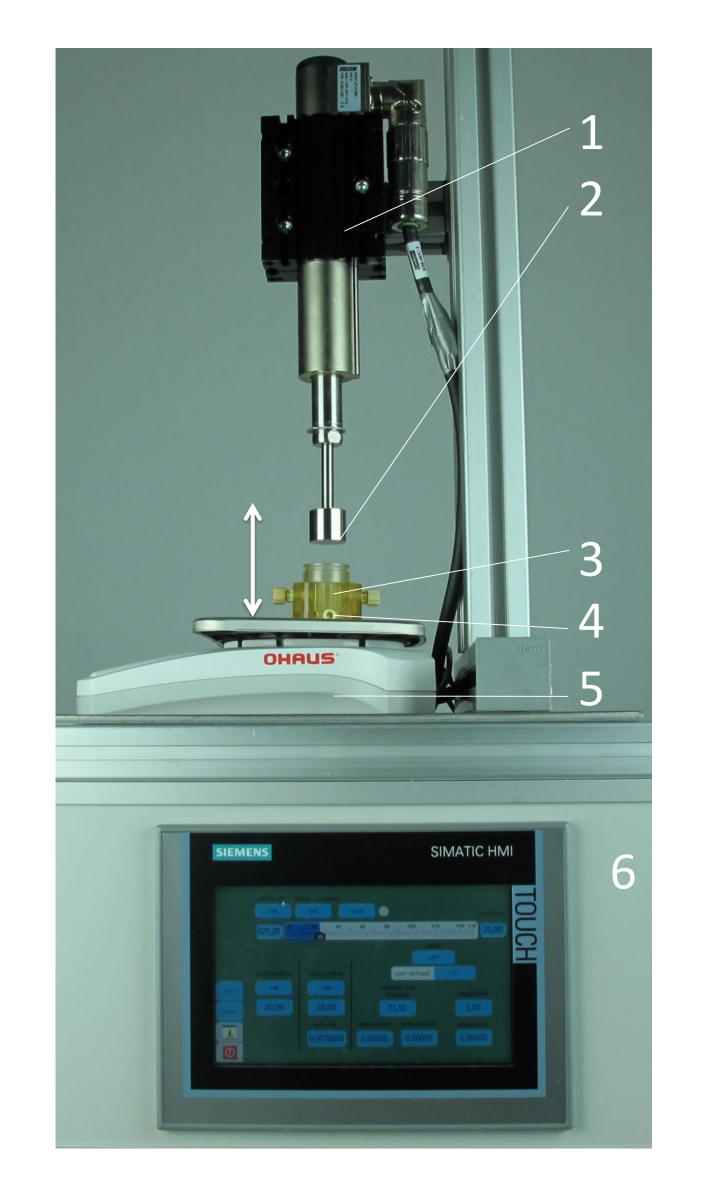






#### higher reproducibility level.

### Results



Plastic

hydrogels

adjustable collagen concentrations.

hydrogels are compressed to a

employing a linear motion engine

(1). The squeezer (2) compresses

bioreactor. Surplus water was

drained via the access near the

bottom of the chamber (4). The

scale allows force measurements

hydrogel (3) occupying the

hydrogel

allowing generation of

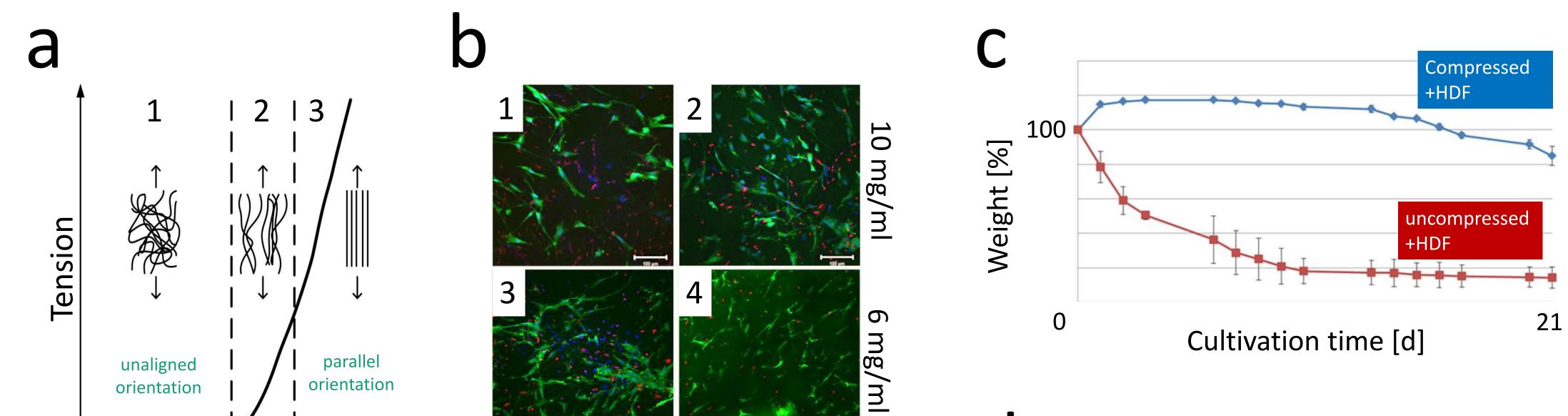
volume of V=3.6 cm<sup>2</sup>

compression

exhibiting

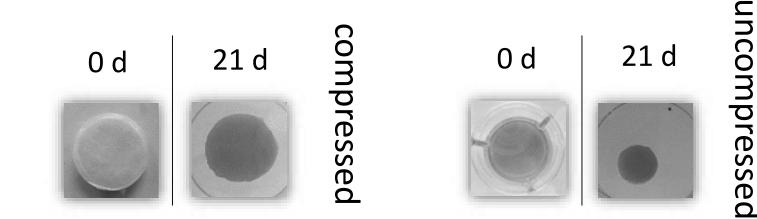
processing,

Using the plastic compression system (Fig. 1) we obtained assimilation towards the mechanical properties of *ex vivo* dermis samples (Fig. 2a) together with an absence of self-contraction (Fig. 2c,d). Moreover, we were able to generate models with a topographical surface structure using the plastic compression system in order to mimic the human papillary structure (results not shown). After compression, the survival of primary fibroblasts, seeded into the collagen hydrogel, was identified by MTT and live dead staining (Fig. 2b).



Strain

Image: Note of the state of the st



**Figure 2: (a)** Tension– strain– diagram of the dermal fiber network during force transmission, adapted by [1]. By carrying out pressure onto the uncompressed hydrogels, the unaligned collagen fibers (1) get a higher degree of parallel orientation (2). This leads in fact to a direct action of the forces from the squeezer onto the collagen fibers that get orientated completely parallel (3). (b) Three dimensional LSM images displaying collagen hydrogels containing human dermal fibroblasts (HDF) at a depth of 60 - 100  $\mu$ m after 17 days of cultivation. A life- dead staining was performed using Hoechst 33342 (blue) for nuclei, fluorescein diacetate (FDA, green) for metabolic active cells und propidium iodide (PI, red) for dead cells. The LSM images display compressed (1, 3) and not compressed (2, 4) collagen hydrogels that were cultivated with HDF. Images 1 and 2 show hydrogels concentrated at c=10mg/ml, images 3 and 4 display hydrogels with a lower concentration of c=6mg/ml. All scale bars indicate 100  $\mu$ m. (c) Weight progression of compressed hydrogels show a shrinking of appr. 70 % compared to initial state. The recorded curves display the mean and standard deviation of three individual samples. (d) Images of the shrinking rate with and without compression of the collagen hydrogels with HDF at a concentration of c=6mg/ml. Not compressed gels show a clear shrinking of appr. 70% compared to compressed gels that only display a minor shrinking rate.

### Summary

Figure

system

collagen

During

defined

the

(5)

1:

The established bioreactor system was proven to be capable of both compression and culturing *in vitro* skin equivalents. Compression nearly cuts down the shrinking process of the models thereby enabling a good attachment of the epidermal layer as there is no shriveling of the dermis. This is especially useful when looking at the production of 3d skin models with an epidermal layer. We also showed that the plastic compression process does not harm the viability of the human dermal fibroblasts. In both processes, more orientated collagen fibers and a structured surface of the models are able to mimic the *in vivo* situation even better in order to perform testing closely related to the human skin and its compartments.

## Outlook

In our study we established a bioreactor for optimizing both compression and culturing *in vitro* skin equivalents. The system can, in perspective, be

used for cultivation of test systems under perfusion to mimic the *in vivo* situation with stable nutrition supply.

# References

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